ABSTRACT

Miniature, lightweight, miser actuators that operate similar to biological muscles can be used to develop robotic devices with unmatched capabilities and impact many technology areas. Electroactive polymers (EAP) offer the potential to producing such actuators and their main attractive feature is their ability to induce relatively large bending or longitudinal strain. EAP actuators can change the paradigm about the complexity of robots, where robotic components such as motors, gears, bearings, and others can be eliminated with simple drive mechanisms. Generally, these materials produce a relatively low force and the applications that can be considered at the current state of the art are relatively limited. While improved material are being developed there is a need for methods to develop longitudinal actuators that can contract similar to muscles. In this study, the authors began investigating the electromechanical behavior of polymers in reaction to a complex configuration of electric fields. A computer model was used to simulate the electromechanical response. Efforts were made to develop both the material basis as well as the electromechanical modeling of the actuator.

Keywords: Miniature Robotics, Electroactive Polymers, EAP Actuators

1. INTRODUCTION

Efficient miniature actuators that are light, compact and driven by low power are needed to drive telerobotic devices and space mechanisms in future NASA missions. Actuators that are driven by transduction phenomena, where electrical, thermal or magnetic signals are converted into a displacement or strain have already, are increasingly finding applications in planetary mechanisms. Electroceramics (EAC) offer effective, compact, actuation materials and they are incorporated into such mechanisms as ultrasonic motors, inchworms, translators and manipulators. Also, Shape Memory Alloys (SMA) are finding applications where low speed, large force actuation at <4% strain actuation is needed. In contrast to EAC and SMA, electroactive polymers (EAP) are emerging as new actuation materials (Furukawa and Wen, 1984) with displacement capabilities that cannot be matched by the striction-limited and rigid ceramics. EAPs are lighter and their displacement actuation capability can be as high as two orders of magnitude more than EACs (Bar-Cohen, et al., 1998). Further, their response speed is significantly higher than Shape Memory Alloys (SMAs). Polymers actuators offer unique capabilities that are the result of their resilience, fracture toughness, large actuation strain constant, inherent vibration damping and tailorable properties (Bar-Cohen, et al., 1997; Hunter and Lafontaine, 1992; and Kornblush, et al., 1995). Generally, once their ability to induce large force is sufficiently enhanced they can be designed to emulate the operation of biological muscles.

The development of actuators that emulate muscle is involved with interdisciplinary efforts using expertise in materials science, chemistry, electronics, and robotics. The infrastructure of this field is still lack key technologies and capabilities that need sufficient progress before such actuators can be used for such applications as augmenting handicap mobility. EAP materials can be categorized in mostly two groups including (a) bending actuators and (b) longitudinal actuators. The emphasis of this manuscript is on the longitudinal EAP actuators with emphasis on electrostatically activated EAPs. In parallel to the authors research effort to develop efficient materials, they are seeking to identify robotic and planetary applications in NASA future missions to transfer the technology. Beside the design of mechanisms where the EAP actuators can be employed while accounting for their deficiencies, a study is underway to develop computer control capability for remote operation. An important issue that needs adequate attention is the current lack of effective sensors that are flexible and lightweight to provide feedback data for robotic tasks actuated by EAP materials.
2. LONGITUDINAL ELECTROSTATIC POLYMER ACTUATORS

Polymers with low elastic stiffness and high dielectric constant can be used to induce large actuation strain by subjecting the material to an electrostatic field. These characteristics of polymers allow producing longitudinal actuators that operate similar to biological muscles using Coulomb forces between electrodes to squeeze or stretch the material. Traditional electrostatic actuators are fabricated as a capacitor with parallel electrodes with a thin air gap between them. One of the major disadvantages of this type of actuators is their relatively low breakdown voltage and they are producing longitudinal extension rather than contraction. The authors adopted the approach that was reported by Kornsluh, et al, 1998, where a longitudinal electrostatic actuator is made of dielectric elastomer film coated with carbon electrodes. The force (stress) that is exerted normally on such a film with compliant electrodes is as follows:

\[ P = \varepsilon_0 E^2 = \varepsilon_0 \varepsilon_r (V/t)^2 \]  

(1)

Where: \( P \) is the normal stress, \( \varepsilon_0 \) is the permittivity of vacuum and \( \varepsilon_r \) is the relative permittivity (dielectric constant) of the material, \( E \) is the electric field across the thickness of the film, \( V \) is the voltage applied across the film and \( t \) is the thickness of the film.

Examining the equation above, it is easy to notice that the force magnitude is twice as large as that for the case of rigid parallel electrodes. To obtain the thickness strain the force needs to be divided by the elastic modulus of the film. Use of polymers with high dielectric constants and application of high electric fields induces large forces and strains. To obtain the required electric field levels one needs to either use high voltage and/or employ thin films. For elastomers with low elastic modulus, it is reasonable to assume a Poisson’s ratio of 0.5. This means that the volume of the polymer is kept constant while the film is deformed under the applied field. As a result, the film is squeezed in the thickness direction causing expansion in the transverse plane. For a pair of electrodes with circular shape, the diameter and thickness changes can be determined using the following relation, where the second order components are neglected.

\[ \frac{\Delta D}{D_0} = -(1/2)\frac{\Delta t}{t_0} \]  

(2)

Where: \( D_0 \) is the original diameter of the electrodes and \( \Delta D \) is the resultant diameter change, \( t_0 \) is the original thickness and \( \Delta t \) is its change under electric activation.

Thus, polymers with a low elastic modulus and a high dielectric constant exhibit large strain under electrical stimulation and they can potentially serve as materials for longitudinal EAP. Some candidate polymers [Kornsluh, et al, 1998] are listed in Table 1.

<table>
<thead>
<tr>
<th>Polymer Type</th>
<th>Energy Density (J/cm³)</th>
<th>Pressure (MPa)</th>
<th>Strain (%)</th>
<th>Young's Modulus (MPa)</th>
<th>Maximum Electric Field (V/μm)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Polyurethane, Deerfield PT61 00S</td>
<td>0.10</td>
<td>1.9</td>
<td>11</td>
<td>17.0</td>
<td>160</td>
</tr>
<tr>
<td>Silicone Dow Corning Sylgard 186</td>
<td>0.034</td>
<td>0.21</td>
<td>32</td>
<td>0.7</td>
<td>144</td>
</tr>
<tr>
<td>Fluorosilicone Dow Corning 730</td>
<td>0.019</td>
<td>0.070</td>
<td>28</td>
<td>0.5</td>
<td>80</td>
</tr>
<tr>
<td>Fluorodastomer Laurenl-143HC</td>
<td>0.0080</td>
<td>0.20</td>
<td>8</td>
<td>2.5</td>
<td>32</td>
</tr>
<tr>
<td>Polybutadiene Adrich PBD</td>
<td>0.011</td>
<td>0.19</td>
<td>12</td>
<td>1.7</td>
<td>76</td>
</tr>
<tr>
<td>Isoprene Natural Rubber Latex</td>
<td>0.0052</td>
<td>0.094</td>
<td>11</td>
<td>0.85</td>
<td>67</td>
</tr>
</tbody>
</table>

To produce a longitudinal actuator with large actuation force, a stack of two silicone layers (Dow Corning Sylgard 186) was used with carbon electrodes on both sides of one of the layers. The displacement in the rope cross section is a rotational one around the rope axis and it is constrained by interlaminar stresses. Therefore, the total actuation extension of the rope is proportional to its length and the resultant actuation force is proportional to the cross-section area normal to the axis. To develop an EAP muscle using such a rope, the length and diameter are used as design parameters, enabling the adaptation of the rope actuator to specific applications. In Figure 1, a silicone film is shown to produce about 12% extension at 2500-V and in a rope form it is used to drop and lift a 10-g rock with displacement of about 6%.
3. ROBOTIC APPLICATIONS USING EAP ACTUATOR

The availability of EAP actuators that can bend or extend/contract allows producing unique robotic devices that emulate human hands. The JPL authors investigated several potential applications for the ESSP type EAP and a robotic arm was developed with a gripper end effector. A computer program was developed using MATLAB computer code that allowed the control of the lifting and dropping of the arm as well as the operation of the end effector as shown in Figure 2. The miniature lightweight robotic arm shown in this Figure was actuated by a longitudinal EAP based on a rolled thin silicone film in the form of a rope. A model of the arm was computer simulated first to select an effective configuration for its construction as shown on the top section of Figure 2. A 5-mm diameter graphite/epoxy rod was used as the base arm and an ESSP rope was connected on the short end of this balanced rod and was used to lower and raise the arm as shown in Figure 2. On the right of the rod a gripper was mounted as an end effector using bending EAP fingers and miniature hooks to secure the gripped objects. The rope was consisted of a silicone film and it required voltage levels of 30-70 V/µm, which reached between 1 and 2.5-KV to produce the levels of several percents actuation strain (shown in Figure 1). Since the film is squeezed as a result of the activation, it becomes longer under the electro activation making the rope longer. This longitudinal EAP rope actuated the arm by tilting its balance and the lifting displacement is determined by the ratio between its connection distance from the pivot point compared to the gripper distance. The longitudinal EAP was used here as the equivalent of human muscle with the exception that it becomes longer under activation. To allow performing tasks with this robotic arm, a gripper end-effector was developed. This gripper that is described in more details by [Bar-Cohen, et al, 1998] has four fingers to grab and hold objects and operate similar to the human hand. The inability of the bending EAP to lift any significant mass was taken into account in this application by avoiding this necessity. The fingers, which have remarkable opening capability, were used to "hug" the samples and grab on them by hooks that attached at the finger bottom. The fingers move back and forth opening and closing the gripper similar to human hand, embracing the desired object and gripping on it. The hooks at the end of the fingers are functioning similar to fingernails to hold the object securely. The gripper was driven by 2 to 5-V signals at a frequency of 0.1-Hz to induce large displacements, because the actuated stair drops with the increase in frequency. The robotic arm was programmed such that it is lowered near the object to be collected, then the gripper fingers are opened as the arm comes down and allowed to close on the object and holding it with aid of the hooks. At this point the fingers are closed and the object is lifted. The demonstration of this robotic arm and gripper capability to lift a rock was intended to pave the way for a future application to planetary sample collection tasks providing miniature ultra-dexterous and versatile tool.

4. COMPUTER AIDED SIMULATION

In order to be able to control a longitudinal EAP to perform complex tasks, the authors investigated the ability to manipulate the electric field within the polymer. The displacement due to applied electrostatic actuation has been characterized using a mixed-domain computer aided simulation tool - MEMCAD software (Microcosm Inc., Cambridge, MA). The result of the displacement matches well with experimental data. A schematic configuration showing the response of a film with parallel
electrodes both and a sketch simulation are shown in Figure 3. The response to the electric field was exaggerated to help visualize the reaction of the polymer. Generally, the electric field cannot be raised above the breakdown voltage and this set the limit to the maximum expected contraction of the plate. The electrodes are drawn away from the film edge to illustrate the efforts to minimize the effect of the low breakdown voltage in air. An example of a complex electroding configuration and the resultant electric field is shown schematically in Figure 4.

Figure 2: A simulated view (top) and a constructed robotic arm, which takes advantage of the capability of longitudinal and bending EAP actuators.

Figure 3: A schematic view of an ESSP actuator using a thin film with parallel electrodes.

Figure 4: The electric field in a patterned electroding configuration demonstrating the potential of field manipulation.

6. CONCLUSION

Electroactive polymers are showing a superior actuation displacement, mass, cost, power consumption and fatigue characteristics over conventional electromagnetic, EAC and SMA actuators. Two type actuation materials have emerged in recent years inducing bending and longitudinal actuation displacement. The longitudinal EAP actuators are important family of materials that has the most potential to emulate biological muscles. Key elements of making such materials as the actuators of choice in the future is the development of material with enhanced force actuation and the ability to theoretical
model complex configurations. The ability of such material to support miniature robotics was demonstrated by the JPL authors who developed a miniature lightweight robotic arm and controlled its performance via computer. This robotic arm was constructed similar to human hand using a composite rod and a scrolled rope electrostatic actuator for the lifting mechanism and a 4-finger gripper as an end-effector. The force actuation capability of EAPs is limited, their actuation displacement levels are unmatched. The longitudinal displacement actuation was obtained using electro-statically-activated films that were rolled to form ropes and served as the equivalence of biological muscles. To enable complex operations using such EAP actuators efforts were initiated to computer model and simulate the electro-activation behavior.

7. ACKNOWLEDGEMENT

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8. REFERENCES


